

Francesca Berti¹, Dario Allegretti¹, Carlo Guala¹, Francesco Migliavacca¹, Giancarlo Pennati¹ and Lorenza Pettrini²

¹ LaBS, Chemistry, Materials and Chemical Engineering Department, Politecnico di Milano

² Department of Civil and Environmental Engineering, Politecnico di Milano

INTRODUCTION

Occlusion of peripheral arteries

Restore the original lumen area
Give support to the vessel during healing

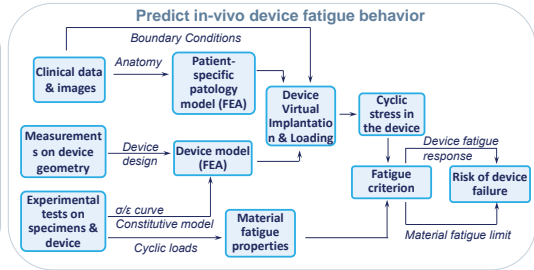
Cyclic loads e.g. leg movements

Multi-axial & non-proportional state of stress and strain in the device

Fatigue failure and other possible complications (e.g. in-stent-restenosis)

Fatigue analysis is one of the requirements of regulatory bodies for the pre-clinical validation of stents

In-vivo loading conditions are replicated in complex simulations



MATERIALS AND METHODS

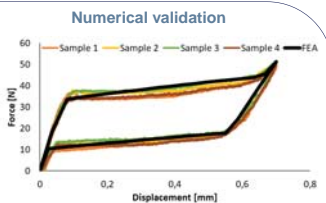
Experimental tests

Identification of material parameters on material multi-wires specimens

Axial tensile test on 6 multi dog-bone specimens (temperature controlled chamber 37°C, strain rate < 0.0002 sec⁻¹)

Finite Element models

Finite element analysis of the specimen geometry to obtain the set of parameters for the SMA constitutive ANSYS material



Comparison of different prediction fatigue criteria^[1,2]

Criterion for proportional loadings based on equivalent strain

Von Mises Alternate Strain

$$\epsilon_{VM}^M = \frac{1}{(1+n)^2} \sqrt{(\epsilon_{11}^{max} - \epsilon_{11}^{min})^2 + (\epsilon_{22}^{max} - \epsilon_{22}^{min})^2 + (\epsilon_{33}^{max} - \epsilon_{33}^{min})^2}$$

Criteria for non-proportional loadings based on the critical plane

Fatemi-Socie

$$FS = \frac{\sigma_{max}}{2} \cdot (1 + K \cdot \frac{\sigma_{max}}{\sigma_y})$$

Smith-Watson-Topper

$$SWT = \sigma_{n,max} \cdot \epsilon_{n,max}^2$$

Brown-Miller

$$BM = \gamma_n^{max} + S_e \epsilon_{n,max}$$

The Critical Plane in a polar coordinate system is where the stress responsible of the crack propagation takes the maximum value.

Identification of devices static response

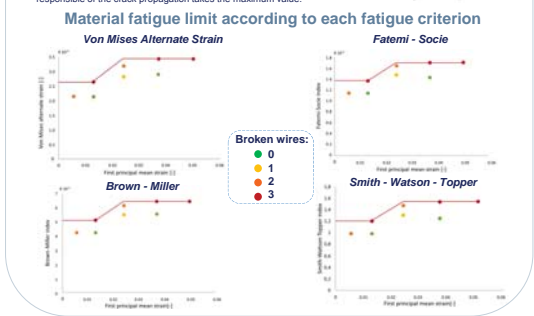
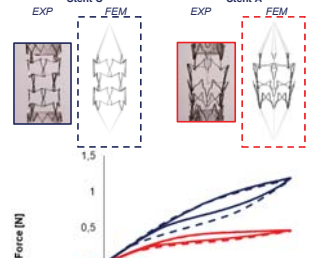
Stent C Peak-To-Peak
Stent A Peak-To-Valley

FE Stent C model

203600 8-node cubic elements

FE Stent A model

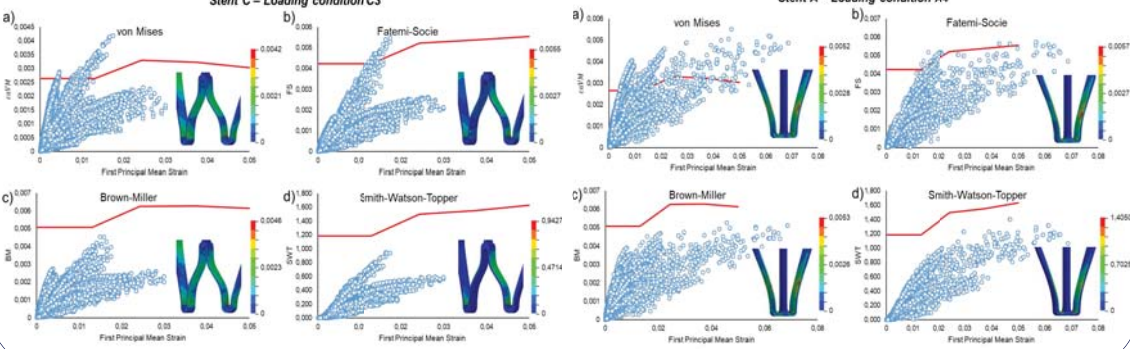
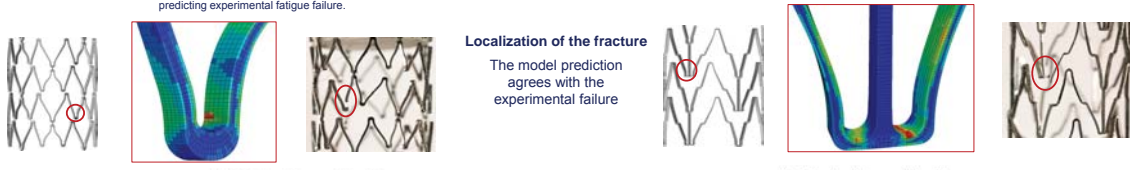
196890 8-node cubic elements



RESULTS

Stent C							Stent A							
Loading [mm]		Fatigue Criteria Prediction				Experimental Outcome	Loading [mm]		Fatigue Criteria Prediction				Experimental Outcome	
Mean	Amplitude	VM	F-S	B-M	S-W-T		Mean	Amplitude	VM	F-S	B-M	S-W-T		
(1)	2.25	0.25	P	P	P	P	-	1.65	0.15	P	P	P	P	-
(2)	2.3	0.3	B-F	P	P	P	-	1.75	0.25	B-F	P	P	P	-
(3)	2.425	0.425	F	F	P	P	2 exp (P-P)	1.85	0.35	F	B-F	P	P	2 exp (P-P)
(4)	2.5	0.5	F	F	B-F	B-P	3 exp (F-P-F)	1.9	0.4	F	F	P	P	3 exp (F-P-F)
(5)	2.525	0.525	F	F	F	B-F	2 exp (F-F)	1.95	0.45	F	F	B-F	B-F	2 exp (F-F)
(6)	2.6	0.6	F	F	F	F	2 exp (F-F)							

B-M and S-W-T approaches seem to be more reliable in predicting experimental fatigue failure.



Extension on a different case study: NiTi stent frame of Aortic valve analysis

TAVI: Transcatheter Aortic Valve Implantation

In durability tests, the valve is implanted in a silicone compartment and subjected to cyclic blood pressure^[3].

CONCLUSIONS

• **INDUSTRY**
Design & Optimization

Possible applications:

• **CLINICS**
Postoperative follow-up
Preoperative planning

• **ACADEMIA**
Upgrade in the State of the Art

✓ **Brown-Miller and Smith-Watson-Topper** criteria seem to give the most accurate fatigue prediction whereas Von Mises equivalent strain and Fatemi-Socie criteria overestimate the risk of failure

? The methodology should be applied to more devices in different loading conditions.

? Others fatigue criteria (e.g. Dang Van) should be considered